

## Voltammetric Determination of Glutathione in Pharmaceutical and Biological Samples Using Multiwall Carbon Nanotubes Paste Electrode in the Presence of Rutin as a Mediator

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### Abstract

A new sensitive and selective electrochemical sensor was developed for electrocatalytic determination of glutathione (GSH) in pharmaceutical and biological samples. GSH is a tripeptidethiol present in all eukaryotic and probiotic cells. A voltammetric study of GSH has been carried out at the surface of carbon paste electrode modified with multiwall carbon nanotubes in the presence of rutin as a mediator. The electrochemical oxidation of GSH was investigated by cyclic voltammetry, chronoamperometry and square wave voltammetry (SWV) techniques. Under the optimized conditions, the peak current was linear to GSH concentration over the concentration range of 0.3 to 180  $\mu\text{mol L}^{-1}$  using SWV. The detection limit was 0.09  $\mu\text{mol L}^{-1}$ . The proposed method was successfully applied to the determination of GSH in the urine, tablet and hemolysed erythrocyte samples.

**Keywords:** Glutathione; Rutin; Multiwall carbon nanotubes; Modified electrode; Voltammetry.

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### Introduction

Electrochemical sensing based on carbon nanotubes (CNTs) is now a developed research field. Several advantages of CNTs as electrode materials have been attested for analysis of diversified chemicals of food quality, pharmaceutical and environmental interest (1-3). CNT-modified sensors exhibit low limit of detection (LOD) and fast response due to the signal enhancement provided by high surface area, low overvoltage, and rapid electrode kinetics (4,5). A thermal conductive, mechanically strong and chemically stable nature of CNTs is very appealing for sensing

applications (6-8). Their high surface-to-volume ratio of nano-materials and especially carbon nanotubes is also a definite asset toward the development of electrochemical platforms for electro-active compounds detection (9-15).

Drug analysis plays important roles in drug quality control, and has a great impact on public health (16-21). Therefore, a simple, sensitive and accurate method for the determination of active ingredient is very important.

Biological thiols, such as glutathione (GSH) occur widely in living tissues. GSH is the most abundant low molecular mass thiol found in cells. GSH plays a vital role in human metabolism, including the detoxification of xenobiotics, cell homeostasis, radioprotection and antioxidant defense (22). Newly, it has been reported that

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GSH is incorporated into certain proteins in response to oxidative stress and may participate in posttranslational protein modification (23). So, determination of this compound is important in biological and pharmaceutical samples. The objective of this research is to develop a novel, sensitive, selective and simple electrochemical method with good reproducibility and repeatability for the determination of GSH using unique properties of MWCNTs as a sensor and rutin as a mediator.

## Experimental

### *Apparatus and reagents*

All the voltammetric measurements were performed using an AutolabPGSTAT 302N, potentiostat/galvanostat (Utrecht, The Netherlands) connected to a three-electrode cell, Metrohm (Herisau, Switzerland) Model 663 VA stand, linked with a computer (Pentium IV, 1,200 MHz) and with Autolab software. A platinum wire was used as the auxiliary electrode. MWCNTPE and Ag/AgCl/KCl<sub>sat</sub> were used as the working and reference electrodes, respectively. The electrode prepared with carbon nanotubes was characterized by scanning electron microscopy (SEM) (Seron Tech. AIS 2100). A digital pH/mV-meter (Metrohm model 710) was applied for pH measurements. Spectrally pure graphite powder (particle size < 50 μm) from Merck and multiwall carbon nanotubes (> 90% MWCNTs basis, d × l = (110–70 nm) × (5–9 μm) from Fluka were used as the substrate for the preparation of the carbon paste electrode.

### *Preparation of the electrode*

Graphite powder (0.900 g) was dissolved in diethyl ether and hand mixed with 0.100 g carbon nanotubes in a mortar and pestle. The solvent was evaporated by stirring. A syringe was used to add paraffin to the mixture, which was mixed well for 40 min until a uniformly wetted paste, was obtained. The paste was then packed into a glass tube. Electrical contact was made by pushing a copper wire down the glass tube into the back of the mixture. When necessary, a new surface was obtained by pushing an excess of the paste out of the tube and polishing it on a weighing paper.

### *Preparation of real samples*

For preparation of tablet solution, five tablets of glutathione, labelled 100mg per tablet (Chongqing Yaoyou Pharmaceutical Co., Ltd.). Then, 10mg of each tablet powder was accurately weighed and dissolved in 100mL water by ultrasonication. After mixing completely, the mixture was filtered on an ordinary filter paper, 10 mL of which was subsequently transferred into a 100-mL volumetric flask and diluted to the mark with water. Then, 1.0mL of the solution plus 4.5ml of the buffer (pH 5.0) was used for analysis using the standard addition method.

The urine samples were taken from humans and were used for measurements after its centrifuged (2,500 rpm, 25 °C) and diluted two times with water without any further pretreatment. The standard addition method was used for the determination of the GSH contents after dilution of the sample.

Human whole blood samples were obtained from the Isfahan University Health Centre. Erythrocytes/erythrocyte was prepared according to reported procedure (24).

### *Optimization of rutin concentration*

The influence of rutin concentration on the peak currents was studied in the concentration range of 0.5-3.0mmol L<sup>-1</sup> rutin at pH = 4.0. The results showed that by increasing the rutin concentration up to 1.0mmol L<sup>-1</sup> the net peak current increased, whereas further increasing the concentration of rutin caused a decrease in the magnitude of the peak current. Therefore, 1.0 mmol L<sup>-1</sup> was selected as the optimal rutin concentration.

## Results and Discussion

### *SEM characterization*

Figure 1 shows SEM images for MWCNTPE and CPE. Result shows, at a surface of CPE (Figure 1A), the layer of irregularly flakes of graphite powder were present and isolated with each other. After multiwall carbon nanotubes (MWCNTs) added to carbon paste matrix, it can be seen that MWCNTs were distributed on the surface of electrode with special three-dimensional structure (Figure 1B), indicating that the MWCNTs were successfully modified on the MWCNTPE.

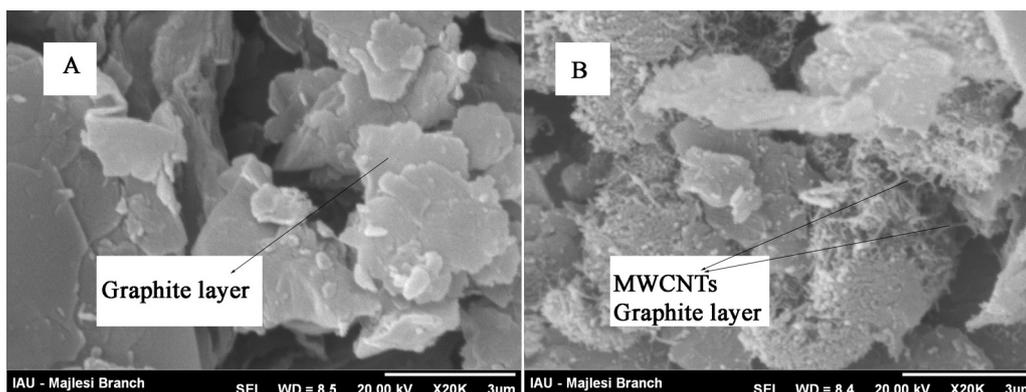


Figure 1. SEM image of a) CPE, b) MWCNTPE.

### Electrochemistry of rutin

The cyclic voltammograms of rutin at a surface of MWCNTPE in  $0.04 \text{ mol L}^{-1}$  universal buffer (pH = 4.0) are shown in Figure 2. In set. As can be seen, the cyclic voltammogram exhibits an anodic peak at the forward scan of the potential related to the oxidation of the rutin<sub>(red)</sub> to rutin<sub>(ox)</sub>. In the reverse scan of the potential, a cathodic peak appears related to the reduction of rutin<sub>(ox)</sub> to rutin<sub>(red)</sub>. A pair of quasi-reversible

peaks are observed at  $E_{pa} = 0.50 \text{ V}$  and  $E_{pc} = 0.33 \text{ V}$  vs. Ag/AgCl. The half-wave potential ( $E_{1/2}$ ) was  $0.43 \text{ V}$  vs. Ag/AgCl and  $\Delta E_p$  ( $E_{pa} - E_{pc}$ ) was  $0.17 \text{ V}$ . The electrode process was quasi-reversible, with  $\Delta E_p$ , greater than the expected value ( $59/\text{nmV}$ ) for a reversible system. The plot of the anodic peak current was linearly dependent on  $v^{1/2}$  for all scan rates (Figure 2). This behavior indicates that the nature of the redox process is diffusion controlled.

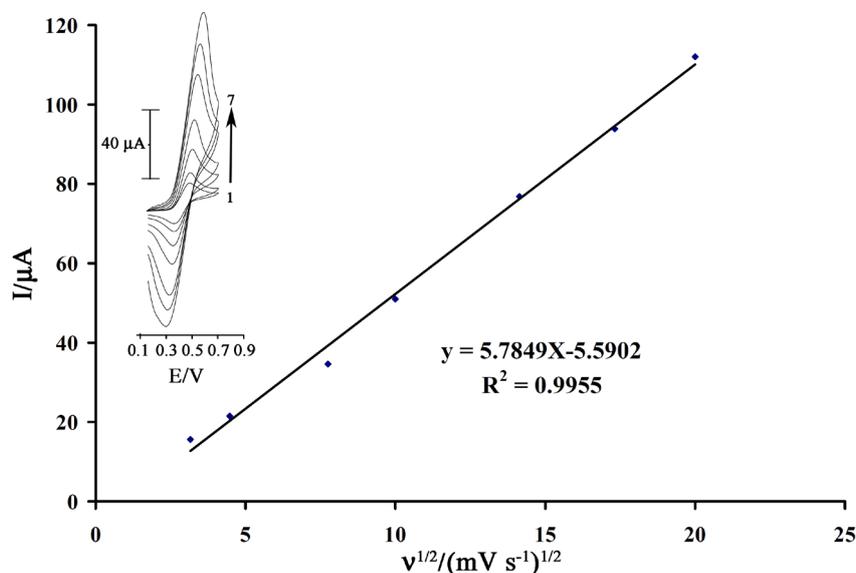


Figure 2. Plot of  $I_{pa}$  versus  $v^{1/2}$  for the oxidation of  $1.0 \text{ mmol L}^{-1}$  rutin at a surface of MWCNTPE. Insert cyclic voltammograms of at various scan rates: (1) 10; (2) 20; (3) 60; (4) 100; (5) 200; (6) 300 and (7)  $400 \text{ mV s}^{-1}$  in  $0.04$  universal buffer (pH = 4.0).

The active surface areas of the modified electrodes are estimated according to the slope of the  $I_p$  vs.  $v^{1/2}$  plot for a known concentration of  $\text{K}_2\text{Fe}(\text{CN})_6$ , based on the Randles-Sevcik equation (25):

$$I_p = 2.69 \times 10^5 n^{3/2} A D_R^{1/2} v^{1/2} C_0 \quad (1)$$

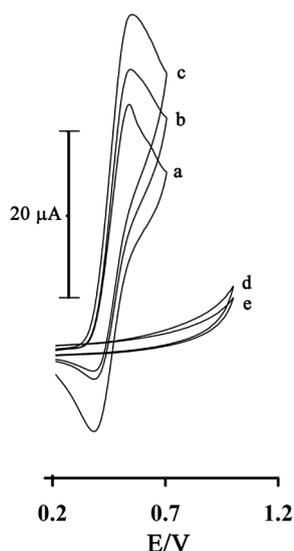
Where  $I_{pa}$  refers to the anodic peak current,  $n$  the electron transfer number,  $A$  the surface area of the electrode,  $D_R$  the diffusion coefficient,  $C_0$  the concentration of  $\text{K}_2\text{Fe}(\text{CN})_6$  and  $v$  is the scan rate. For  $1.0 \text{ mmol L}^{-1} \text{K}_2\text{Fe}(\text{CN})_6$  in  $0.10 \text{ mol L}^{-1} \text{KCl}$  electrolyte with  $n=1$  and

$D_R = 7.6 \times 10^{-6} \text{ cm}^2 \text{ s}^{-1}$  and from the slope of the  $I_{pa} - v^{1/2}$  relation, the microscopic areas were calculated. The active surface areas were equal to 0.05 and 0.091  $\text{cm}^2$  for CPE, MWCNTPE. The result shows that the presences of MWCNTPE cause increasing the active surface of the electrode.

#### Electrocatalytic investigation of GSH

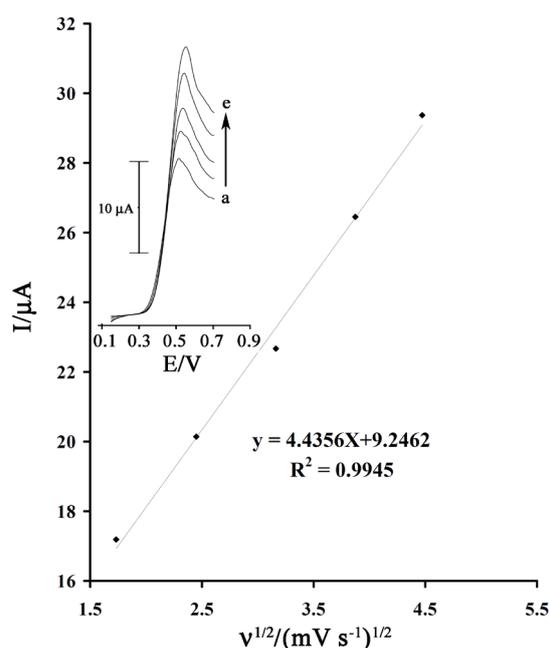
Figure 3 shows the electrocatalytic oxidation of GSH in the presence of rutin at a MWCNTPE surface. As is obvious, at the potential range studied (0.2–1.0 V), GSH was not electroactive at a surface of MWCNTPE and CPE (Figure 3(d and e)), respectively.

On the other hand, the anodic current of rutin was increased substantially in the presence of low concentrations of GSH at a surface of MWCNTPE and CPE (Figure 3(c) and 3(b)), respectively. This observation is an evidence for electrocatalytic oxidation of GSH by rutin. Similarly, when we compared the oxidation of GSH at the surface of MWCNTPE (curve c) and at CPE (curve b) in the presence of mediator, a dramatic enhancement was observed in the anodic peak current at MWCNTPE vs. the value obtained with CPE. In other words, the data obtained clearly show that the combination of MWNTs and the mediator definitely improve the characteristics of the electrode for the oxidation of GSH.



**Figure 3.** Cyclic voltammograms of 1.0 mmol  $\text{L}^{-1}$  rutin at the surface of MWCNTPE in 0.04  $\mu\text{mol L}^{-1}$  universal buffer solution (pH = 4.0) at a scan rate of 20  $\text{mV s}^{-1}$  in the absence (a) and in the presence of 100  $\mu\text{mol L}^{-1}$  GSH (c). (b) as (c) for the carbon paste electrode. (d) as (c) and (e) as (b) in the absence of rutin.

The scan rate dependence of linear sweep voltammograms of a GSH solution (80  $\mu\text{mol L}^{-1}$ ) in the presence of rutin (1.0 mM) was studied (Figure 4 inset) at a MWCNTPE surface. Figure 4 shows that the anodic peak current increases linearly with the square root of the sweep rate as expected for a diffusion controlled reaction. In addition, with increasing potential scan rate, the catalytic oxidation peak potential gradually shifts towards more positive potentials, suggesting a kinetic limitation in the reaction between rutin and GSH.



**Figure 4.** Plot of  $I_{pa}$  versus  $v^{1/2}$  for the oxidation of 80  $\mu\text{mol L}^{-1}$  GSH in the presence 1.0 mmol  $\text{L}^{-1}$  rutin at the surface of MWCNTPE. Inset) Linear sweep voltammograms of 80  $\mu\text{mol L}^{-1}$  GSH in the presence 1.0 mmol  $\text{L}^{-1}$  rutin at various scan rates as 1) 3, 2) 6, 3) 10, 4) 15 and 5) 20  $\text{mV s}^{-1}$  in 0.04  $\mu\text{mol L}^{-1}$  buffer solution (pH = 4.0).

To find further information on the rate determining step, a Tafel plot was developed for the MWCNTPE in the presence of mediator using the data derived from the raising part of the current–voltage curve. The slope of the Tafel plot is equal to  $n(1-\alpha)F/2.3RT$  which comes up to 9.5010  $\text{V decade}^{-1}$ . We obtained  $n_{\alpha}$  as 0.44. Assuming  $n = 1$ , then  $\alpha = 0.44$ .

#### Influence of pH

In order to optimize the electrocatalytic response of the sensor to GSH oxidation, we investigated the effect of solution pH on the

electrocatalytic oxidation of GSH in 0.04 mol L<sup>-1</sup> universal buffer solutions with different pH values (2.0 < Ph < 6.0) using rutin as mediator at a surface of MWCNTPE. The influence of pH on both peaks current and peaks potential were assessed by examining the electrode responses in the buffer solutions. The results show that maximum electrocatalytic current was obtained at pH 4.0. Therefore, a pH value of 4.0 was chosen as the optimum value for the determination of GSH at MWCNTPE in the presence of rutin.

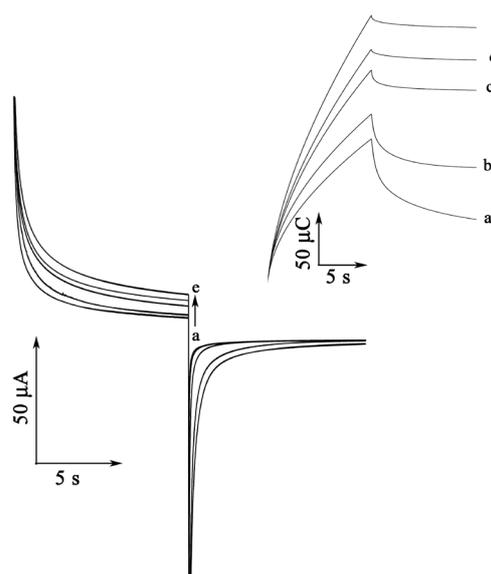
#### Chronoamperometric studies

In order to obtain an estimation of the rate constant of the catalytic oxidation ( $k'_h$ ) of GSH, chronoamperometric method was applied to the system (Figure 5A). The rate constant for the chemical reaction between rutin and GSH ( $k_h$ ) is determined according to the method of Galus (26).

$$I_c/I_L = \pi^{1/2} \gamma^{1/2} = \pi^{1/2} (k_h t)^{1/2} \quad (2)$$

where  $I_c$  is the catalytic current of rutin in the presence of GSH and  $I_L$  is the limiting current in the absence of GSH. From the slope of  $I_c/I_L$  versus  $t^{1/2}$  for five different concentrations of GSH, the average value of  $k_h$  was calculated to be  $8.81 \times 10^2 \text{ M}^{-1} \text{ sec}^{-1}$  (Not shown). This value of rate constant explains the sharp catalytic peak observed for the oxidation of GSH at the surface of MWCNTPE in the presence of mediator.

Figure 5B shows the double-potential step chronocolougrams for the mediator in the absence and presence of different concentration of GSH at a surface of MWCNTPE. The results show that forward and backward potential step chronocoloumetry in a blank buffer solution yields very symmetrical chronocolougrams. These had about an equal charge consumed for both oxidation and reduction of the redox system in the mediator at a surface of MWCNTPE. However, in the presence of GSH, the charge value associated with forward chronocoloumetry was significantly greater than that observed for backward chronocoloumetry. This behavior is typically expected for electrocatalysis at chemically modified electrodes (17-32).



**Figure 5.** A) Chronoamperograms obtained at the MWCNTPE in the absence a) and in the presence of b) 350; c) 450; d) 500 and e) 600  $\mu\text{mol L}^{-1}$  GSH in a buffer solution (pH = 4.0). B) The charge-time curves a') for curve (a); b') for curve (b); c') for curve (c); d') for curve (d) and e') for curve e.

#### Interference studies

Interference studies were carried out with several chemical substances prior to the application of the proposed method for the assay of GSH in hemolysed erythrocyte, urine and tablet. The potential interfering substances were chosen from the group of substances commonly found with GSH in pharmaceuticals and in biological fluids. The influence of various substances as potential interference compounds on the determination of  $5.0 \mu\text{mol L}^{-1}$  GSH under the optimum conditions was studied. Tolerance limit was defined as the maximum concentration of the interfering substance that caused an error less than 5% for determination of GSH. The results are given in Table 1 which shows the peak current of GSH is not affected by all conventional cations, anions, and organic substances.

#### Dynamic range and limit of detection

Square wave voltammetry (SWV) was used to determine the concentration of GSH. The square wave voltammograms clearly showed two linear dynamic ranges that the plot of the peaks current versus GSH concentrations were linear. For  $0.3\text{--}17 \mu\text{mol L}^{-1}$  GSH, the regression equation was  $I_p(\mu\text{A}) = (0.085 \pm 0.003) C_{\text{GSH}} + (2.806 \pm 0.068)$  ( $r^2 = 0.992$ ,  $n = 5$ ) and for

**Table 1.** Interference study for the determination of 5.0  $\mu\text{mol L}^{-1}$  GSH under the optimized conditions.

Species	Tolerance limits (W/W)
$\text{Li}^+$ , $\text{Cl}^-$ , $\text{NO}_3^-$ , Histidine, Alanine, Phenyl alanine, Methionine, Glycine, Methanol, Ethanol, $\text{SCN}^-$ , $\text{SO}_4^{2-}$ , Br <sup>-</sup> , L-Theronine, L-isoleucin, Glucose, Fructose, Lactose, Sucrose, Urea; L_Orinthime, $\text{Ca}^{+2}$ , $\text{Mg}^{+2}$	1000
Starch	Saturation
Ascorbic acid	5

17–180  $\mu\text{mol L}^{-1}$  GSH, the regression equation was  $I_p(\mu\text{A}) = (0.008 \pm 0.001)C_{\text{GSH}} + (4.019 \pm 0.513)$  ( $r^2 = 0.9947$ ,  $n = 8$ ). The detection limit ( $3\sigma$ ) was 0.09  $\mu\text{mol L}^{-1}$ .

The repeatability and stability of the MWCNTPE in the presence of rutin were investigated by cyclic voltammetry measurements of 5.0  $\mu\text{mol L}^{-1}$  GSH. The relative standard deviation (RSD%) for six successive assays was 1.2%. When using five different electrodes, the RSD% for four measurements was 1.9%. When the electrode was stored in our laboratory at room temperature, the modified electrode retained 97% of its initial response after a week and 95% after 30 days. These results indicate

that MWCNTPE in the presence of mediator has both a good stability and a satisfactory reproducibility so that it can be used for GSH determination.

#### *Determination of GSH in real samples*

In order to evaluate the applicability of the modified electrode for measuring GSH in real samples, GSH values in human erythrocyte, tablet, and urine samples were determined using the proposed method. In addition, the results were compared with those obtained from the spectrophotometric method (33) which is usually used as the standard method for GSH determination. The results are reported in Table 2.

**Table 2.** Concentration values obtained from the proposed and Elman methods for GSH analysis in hemolysed erythrocyte, urine and tablet.

Sample	Proposed method ( $\text{mmol L}^{-1}$ )	Elman method ( $\text{mmol L}^{-1}$ )	$F_{\text{ex}}$	$F_{\text{tab}, (0.05); 2; 2}$	$t_{\text{ex}}$	$t_{\text{tab}} (98\%)$
1. Hemolysed erythrocyte	4.45 $\pm$ 0.03	4.48 $\pm$ 0.05	4.5	19	1.8	3.8
2	3.65 $\pm$ 0.08	3.49 $\pm$ 0.10	8.5	19	3.3	3.8
3	5.48 $\pm$ 0.05	5.37 $\pm$ 0.08	6.3	19	2.4	3.8
4	6.01 $\pm$ 0.06	5.98 $\pm$ 0.06	5.5	19	2.0	3.8
5 Urine	<LOD	<LOD	-	-	-	-
6	15.22 $\pm$ 0.41	15.37 $\pm$ 0.41	6.5	19	2.2	3.8
7	30.44 $\pm$ 0.50	30.67 $\pm$ 0.72	7.3	19	2.9	3.8
8 Tablet	5.11 $\pm$ 0.21	5.22 $\pm$ 0.33	4.3	19	1.0	3.8
9	10.23 $\pm$ 0.30	9.88 $\pm$ 0.41	5.2	19	1.5	3.8

$F_{\text{ex}}$  Calculated F-value; Reported F value from F-test table with 95% confidence level and 2/2 degree of freedom;  $t_{\text{ex}}$  Calculated t;  $t_{\text{tab}}$  (98%) Reported t value from t-student test table with 98% confidence level.

#### *Conclusions*

In this study, rutin was used as a mediator for the homogeneous electrocatalytic oxidation of GSH in aqueous media (pH = 4.0) at the surface of a MWCNTPE. The electrochemical characteristics of rutin and its catalytic effect on the oxidation of GSH were investigated. The rate constant of the catalytic reaction was estimated using chronoamperometry. Square wave voltammetry was successfully applied to the determination of GSH in the presence of an

optimum concentration of mediator. Finally, this sensor was used for the determination of GSH in biological and pharmaceutical real samples such as the hemolysed erythrocyte and tablet using standard addition method.

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## References

- (1) Tahernejad-Javazmi, F. Shabani-Nooshabadi, M and Karimi-Maleh H. Analysis of glutathione in the presence of acetaminophen and tyrosine via an amplified electrode with MgO/SWCNTs as a sensor in the hemolyzed erythrocyte. *Talanta* (2018) 176: 208–13.
- (2) Mo Z, Zhang Y, Zhao F, Xiao F, Guo G and Zeng B. Sensitive voltammetric determination of Sudan I in food samples by using gemini surfactant–ionic liquid–multiwalled carbon nanotube composite film modified glassy carbon electrodes. *Food Chem.* (2010) 121: 233-7.
- (3) Beitollahi H, Karimi-Maleh H and Khabazzadeh H. Nanomolar and selective determination of epinephrine in the presence of norepinephrine using carbon paste electrode modified with carbon nanotubes and novel 2-(4-oxo-3-phenyl-3,4-dihydroquinazoliny)-N'-phenyl-hydrazinecarbothioamide. *Anal. Chem.* (2008) 80: 9848-51.
- (4) Merkoci A, Pumera M, Llopis X, Perez B, del Valle M and Alegret S. New materials for electrochemical sensing VI: carbon nanotubes. *Trends Anal. Chem.* (2005) 24: 826-38.
- (5) Rubianes MD and Rivas GA. Carbon nanotubes paste electrode. *Electrochem. Commun.* (2003) 5: 689-94.
- (6) Taheri AR, Mohadesi A, Afzali D, Karimi-Maleh H, Mahmoudi-Moghaddam H, Zamani H and Rezayatizad Z. Simultaneous voltammetric determination of norepinephrine and folic acid at the surface of modified carbon nanotube paste electrode. *Int. J. Electro. chem. Sci.* (2011) 6: 171-80.
- (7) Anik Ü and Çubukcu M. Examination of the electroanalytic performance of carbon nanotube (CNT) modified carbon paste electrodes as Xanthine biosensor transducers. *Turk. J. Chem.* (2008) 32: 711-9.
- (8) Rezaei B and Damiri S. Multiwalled carbon nanotubes modified electrode as a sensor for adsorptive stripping voltammetric determination of hydrochlorothiazide. *IEEE Sen. J.* (2008) 8: 1523-9.
- (9) Safari F, Keyvanfar M, Karimi-Maleh H and Alizad K. Voltammetric determination of penicillamine using a carbon paste electrode modified with multiwall carbon nanotubes in the presence of methyldopa as a mediator. *Iran. J. Pharm. Res.* (2017) 16: 1019-29
- (10) Ensafi AA and Karimi-Maleh H. Voltammetric determination of isoproterenol using multiwall carbon nanotubes-ionic liquid paste electrode. *Drug Test. Anal.* (2011) 3: 325-30.
- (11) Ensafi AA and Karimi-Maleh H. Modified multiwall carbon nanotubes paste electrode as a sensor for simultaneous determination of 6-thioguanine and folic acid using ferrocenedicarboxylic acid as a mediator. *J. Electroanal. Chem.* (2010) 640: 75-83.
- (12) Sanghavi, BJ and Srivastava AK. Adsorptive stripping differential pulse voltammetric determination of venlafaxine and desvenlafaxine employing Nafion–carbon nanotube composite glassy carbon electrode. *Electrochim. Acta* (2011) 56: 4188–96.
- (13) Gadhari NS, Sanghavi BJ, Karna SP and Srivastava A.K. Potentiometric stripping analysis of bismuth based on carbon paste electrode modified with crypt and [2.2.1] and multiwalled carbon nanotubes. *Electrochim. Acta* (2010) 56: 627–35
- (14) Cheraghi S, Taher MA and Karimi-Maleh H. Highly sensitive square wave voltammetric sensor employing CdO/SWCNTs and room temperature ionic liquid for analysis of vanillin and folic acid in food samples. *J. Food Compos. Anal.* (2017) 62: 254–59
- (15) Ashjari M, Karimi-Maleh H, Ahmadpour F, Shabani-Nooshabadi M, Sadrnia A and Khalilzadeh MA., Voltammetric analysis of mycophenolate mofetil in pharmaceutical samples via electrochemical nanostructure based sensor modified with ionic liquid and MgO/SWCNTs. *J Taiwan. Inst. Chem. Eng.* (2017) 80: 989–96
- (16) Yola ML, Eren T and Atar N. Molecularly imprinted electrochemical biosensor based on Fe@ Au nanoparticles involved in 2-aminoethanethiol functionalized multi-walled carbon nanotubes for sensitive determination of cefexime in human plasma. *Biosens. Bioelectron.* (2014) 60: 277-85
- (17) Cheraghi S, Taher MA and Karimi-Maleh H. A sensitive amplified sensor based on improved carbon paste electrode with 1-methyl-3-octylimidazolium tetrafluoroborate and ZnO/CNTs nanocomposite for differential pulse voltammetric analysis of raloxifene. *Appl. Surf. Sci.* (2017) 420: 882–5.
- (18) Karimi-Maleh H, Tahernejad-Javazmi F, Atar N, Yola ML, Gupta VK and Ensafi AA. A Novel DNA biosensor based on a pencil graphite electrode modified with polypyrrole/functionalized multiwalled carbon nanotubes for determination of 6-mercaptopurine anticancer drug. *Ind. Eng. Chem. Res.* (2015) 54: 3634–9.
- (19) Yola ML and Atar N. A highly efficient nanomaterial with molecular imprinting polymer: carbon nitride nanotubes decorated with graphene quantum dots for sensitive electrochemical determination of chlorpyrifos, *J. Electrochem. Soc.* (2017) 164: B223-B229
- (20) Cheraghi S, Taher MA, Karimi-Maleh H and Faghieh-Mirzaei E. A nanostructure label-free DNA biosensor for ciprofloxacin analysis as a chemotherapeutic

- agent: an experimental and theoretical investigation. *New J. Chem.* (2017) 41: 4985-9
- (21) Karimi-Maleh H, Bananezhad A, Ganjali MR and Norouzi P. Electrochemical nanostructure platform for the analysis of glutathione in the presence of uric acid and tryptophan. *Anal. Methods* (2017) 9: 6228–34
- (22) Halliwell B and Gutteridge JMC. *Free Radicals in Biology and Medicine*, 3rd edn., Oxford University Press, Oxford (1999) 146-50.
- (23) Sullivan, DM, Wehr NB, Fergusson MM, Levine RL and Finkel T. Identification of oxidant-sensitive proteins: TNF- $\alpha$  induces protein glutathiolation. *Biochemistry* (2000) 39: 11121-8.
- (24) Ensafi AA, Dadkhah-Tehrani S and Karimi-Maleh H. Voltammetric determination of glutathione in haemolysed erythrocyte and tablet samples using modified-multiwall carbon nanotubes paste electrode. *Drug Test. Analysis* (2011) 3: 325–30
- (25) Bard AJ and Faulkner LR. *Electrochemical Methods, Fundamentals and Applications*, Wiley, New York (2001).
- (26) Galus Z. *Fundamentals of Electrochemical Analysis*, Ellis Horwood, New York (1976).
- (27) Karimi-Maleh H, Keyvanfard M, Alizad K, Khosravi V and Asnaashariisfahani M. Electrocatalytic determination of glutathione using multiwall carbon nanotubes paste electrode as a sensor and isoprenaline as a mediator. *Int. J. Electrochem. Sci.* (2012)7: 6816–30.
- (28) Keyvanfard M, Ensafi AA and Karimi-Maleh H. A new strategy for simultaneous determination of cysteamine in the presence of high concentration of tryptophan using vinylferrocene-modified multiwall carbon nanotubes paste electrode. *J. Solid State Electrochem.* (2012)16: 2949–55.
- (29) Keyvanfard M, Karimi-Maleh H and Alizad K. Multiwall carbon nanotube paste electrode with 3,4-dihydroxy-cinnamic acid as mediator for the determination of glutathione in pharmaceutical and urine, samples. *Chinese J. Catalysis* (2013) 34: 1883–9.
- (30) Keyvanfard M, Sami S, Karimi-Maleh H and Alizad K. Electrocatalytic determination of cysteamine using multiwall carbon nanotube paste electrode in the presence of 3,4-dihydroxycinnamic acid as a homogeneous mediator. *J. Braz. Chem. Soc.* (2013) 24: 32-9.
- (31) Keyvanfard M, Ensafi AA, Karimi-Maleh H and Alizad K. Modified multiwalled carbon nanotubes paste electrode as a sensor for the electrocatalytic determination of N-acetylcysteine in the presence of high concentrations of folic acid. *Anal. Methods* (2012) 4: 3268-76.
- (32) SharifianIsfahani A, Keyvanfard M, Rezaei Band Alizad Kh. Electrocatalytic determination of 6-mercaptopurine using multiwall carbon nanotubes paste electrode in the presence of methyl dopa. *Current Nanoscience* (2014) 10: 512-20.
- (33) Ellman GL. Tissue sulfhydryl groups. *Arch. Biochem. Biophys.* (1959) 82: 70-7.